Skeltal muscle FTU

We consider a 3 compartment voltage regulated/ Ca^{2+} dependent Muscle cell ODE model. This model consists of Ca^{2+} conc. in the SR and the Myofibril space as described in Liu and Olson,2015 coupled with a Ca^{2+} dependent 4 state muscle contraction model as described in Razumova et al,2000.

Calcium Compartment model (Olsen and Liu 2014)

The concentration of free Ca^{2+} in the sarcoplasmic reticulum (SR) is given by

$$\frac{dC_{SR}}{dt} = -R(V) + V_{max}\frac{C_{MS}}{C_{MS} + K_{MS}} - L_p \tag{1}$$

where R(V) is the Ca^{2+} release from the SR that depends on the strength of the nerve stimulation or applied input current and the resulting membrane voltage. Ca^{2+} uptake by SERCA is given by the second term on the rhs of the above equation. The leak parameter to capture the permeability of Ca^{2+} to leak from the SR is given by L_p . C_{MS} represents the concentration of free calcium in the myofibril space and is governed by the following

$$\frac{dC_{MS}}{dt} = R(V) + k_{t2}TC - k_{t1}C_{MS}T + k_{p2}PC - k_{p1}C_{MS}P - V_{max}\frac{C_{MS}}{C_{MS} + K_{MS}} + L_p$$

$$\frac{dTC}{dt} = k_{t1}C_{MS} - k_{t2}TC$$

$$\frac{dPC}{dt} = k_{p1}C_{MS}P - k_{p2}PC$$

We track the concentrations of the proteins and complexes: troponin T, parvalbumin P, troponin-Ca2+ complex TC and parvalbumin-Ca2+ complex PC. The fraction of receptors on the SR calcium release channel that are in an inactivated state is given by (Schneider and Simon, 1988)

$$\frac{dCaR}{dt} = \frac{k_f}{1 + \frac{K}{C_{MS}}} - k_r CaR - CaR \frac{k_f}{1 + \frac{K}{C_{MS}}} \tag{2}$$

The first term on the rhs describes the fraction of receptors that are bound to Ca2+ and transition to the inactivated state CaR. The second term describes inactivated Ca2+ bound receptor and the third term describes Ca2+ unbinding from the receptor. The total Ca^{2+} release from the SR R(V) is given by

$$R(V) = R_{max} \left(\frac{1}{1 + \epsilon_2(1 + \epsilon_1)}\right) (1 - CaR)$$
(3)

where ϵ_i are functions of membrane potential V given by

$$\epsilon_i(V) = e^{\left(\bar{V}_{\epsilon_i} - V\right)/k_{\epsilon_i}} \tag{4}$$

where k and \bar{V} or espond to the steepness factor and mid-point voltage for transition respectively.

Membrane voltage (Olsen and Liu 2014)

The membrane voltahe is modeled by the governing equation

$$C_m \frac{dV}{dt} = -\left(I_{K_f} + I_{K_s} + I_{Na} + I_{Ca} + I_{Cl} + I_{leak}\right) + I_{input} \tag{5}$$

where I_j is the current in channel j, I_{leak} is a generic leak current and I_{input} is an input current.

Potassium current

Two potassium currents are considered a fast (I_{K_f}) and a slow current (I_{K_s}) .

$$I_{K_f} = \bar{g_{k_f}} n^4 \left(V - E_{K_f} \right)$$
$$I_{K_s} = \bar{g_{k_s}} l^2 \left(V - E_{K_s} \right)$$

with gating variables \boldsymbol{n} and \boldsymbol{l} of the form

$$\frac{dn}{dt} = \alpha_n(V)(1-n) - \beta_n(V)n$$
$$\frac{dl}{dt} = \alpha_l(V)(1-l) - \beta_l(V)l$$
$$\alpha_k = \frac{\bar{\alpha_k}(V - \bar{V_k})}{1 - exp\left(-\frac{(V - \bar{V_k})}{\nu_k}\right)}$$
$$\beta_n = \frac{\bar{\beta_n}}{exp\left(\frac{(V - \bar{V_l})}{b_k}\right)}$$
$$\beta_l = \frac{\beta_l(V - \bar{V_l})}{exp\left(\frac{(V - \bar{V_l})}{b_l}\right) - 1}$$

Sodium Current

Parametrers from experiments with striated skeletal muscle fibers were fitted to the standard Huxley sodium current

$$I_{Na} = g\bar{}_{Na}m_{Na}^{3}h_{Na}(V - E_{Na})$$

$$\frac{dm_{Na}}{dt} = \alpha_{m1}(V)(1 - m_{Na}) - \beta_{m1}(V)m_{Na}$$

$$\beta_{m1} = \frac{\beta_{m1}^{-}}{exp\left(\frac{(V - V_{m1})}{b_{m1}}\right)}$$

$$\alpha_{m1} = \frac{\alpha_{m1}^{-}(V - V_{m1})}{1 - exp\left(-\frac{(V - V_{m1})}{\nu_{m1}}\right)}$$

$$\frac{dh_{Na}}{dt} = \alpha_{h1}(V)(1 - h_{Na}) - \beta_{h1}(V)h_{Na}$$

$$\beta_{h1} = \frac{\beta_{h1}^{-}}{1 + exp\left(-\frac{(V - V_{h1})}{b_{h1}}\right)}$$

$$\alpha_{h1} = \frac{\alpha_{h1}^{-}}{exp\left(\frac{(V - V_{h1})}{\nu_{h1}}\right)}$$

Calcium current

Calcium channel kinetics is based in the model of Sanchez and Stefani 1970

$$I_{Ca} = g\bar{c}_{a}m_{Ca}^{3}h_{Na}(V - E_{Na})$$

$$\frac{dm_{Ca}}{dt} = \alpha_{m2}(V)(1 - m_{Ca}) - \beta_{m2}(V)m_{Ca}$$

$$\beta_{m2} = \beta_{m2}^{-}exp\left(\frac{(\bar{V}_{m2} - V)}{b_{m2}}\right)$$

$$\alpha_{m2} = \frac{\alpha_{m2}(V - \bar{V}_{m2})}{1 - exp\left(\frac{(\bar{V}_{m1} - V)}{\nu_{m2}}\right)}$$

$$\frac{dh_{Ca}}{dt} = \alpha_{h2}(V)(1 - h_{Ca}) - \beta_{h2}(V)h_{Ca}$$

$$\beta_{h1} = \frac{\beta_{h2}}{1 + exp\left(\frac{(\bar{V}_{h2} - V)}{b_{h2}}\right)}$$

$$\alpha_{h2} = \alpha_{h2}exp\left(\frac{(\bar{V}_{h2} - V)}{\nu_{h2}}\right)$$

Chlorine current

The chlorine current is modelled by

$$I_{Cl} = \bar{g_{Cl}} \left(\nu_{Cl} + \frac{1 - \nu_{Cl}}{1 + exp\left(\frac{V_{Cl} - V}{k_{Cl}}\right)} \right) (V - E_{Cl})$$

$$\tag{6}$$

The generic leak current is represented by

$$I_{leak} = g_{leak} \left(V - E_{leak} \right). \tag{7}$$

Finally the input current is given by

$$I_{input} = \begin{cases} I_{app} & t_{on} \le t \le t_{off} \\ 0 & otherwise \end{cases}$$
(8)

All parameters can be found in the original paper.

Contractile mechanism (Razumova et al 2000)

We adopt the reduced 4-state representation of the 8-state myofilament activation and crossbridge cycling model. This can be modelled by the following system

$$\frac{dD}{dt} = k_{on}R_{off} - k_{off}D + g_sA_2 + gA_1 - fD$$
$$\frac{dA_1}{dt} = fD + h_2A_2 - gA_1 - h_1A_1$$
$$\frac{dA_2}{dt} = h_1A_1 - h_2A_2 - g_sA_2$$

where D, A_1 and A_2 represent the detatched, attached and attached power stroke states respectively. R_{off} represents the off state tropomyosin-troponin regulatory unit, such that cross-bridge contraction is unable to occur. Via conservation of crossbridge units

$$R_{off} = 1 - D - A_1 - A_2. (9)$$

The contractile force $F = A_1 + A_2$ with the fraction of cycling crossbridges that are generating force is given by

$$\lambda_{cyc} = \frac{A_2}{D + A_1 + A_2}.\tag{10}$$

All parameters can be found in the original papers.

References

- [Liu and Olson, 2015] Liu, Weifan, and Sarah D. Olson. "Compartment calcium model of frog skeletal muscle during activation." Journal of theoretical biology 364 (2015): 139-153.
- [Razumova et al, 2000] Razumova, Maria V., Anna E. Bukatina, and Kenneth B. Campbell. "Different myofilament nearest-neighbor interactions have distinctive effects on contractile behavior." Biophysical journal 78, no. 6 (2000): 3120-3137.